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Sleep Spindles and Intelligence: Evidence for a Sexual Dimorphism

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Sleep spindles are thalamocortical oscillations in nonrapid eye movement sleep, which play an important role in sleep-related neuroplasticity and offline information processing. Sleep spindle features are stable within and vary between individuals, with, for example, females having a higher number of spindles and higher spindle density than males. Sleep spindles have been associated with learning potential and intelligence; however, the details of this relationship have not been fully clarified yet. In a sample of 160 adult human subjects with a broad IQ range, we investigated the relationship between sleep spindle parameters and intelligence. In females, we found a positive age-corrected association between intelligence and fast sleep spindle amplitude in central and frontal derivations and a positive association between intelligence and slow sleep spindle duration in all except one derivation. In males, a negative association between intelligence and fast spindle density in posterior regions was found. Effects were continuous over the entire IQ range. Our results demonstrate that, although there is an association between sleep spindle parameters and intellectual performance, these effects are more modest than previously reported and mainly present in females. This supports the view that intelligence does not rely on a single neural framework, and stronger neural connectivity manifesting in increased thalamocortical oscillations in sleep is one particular mechanism typical for females but not males.

Key words: intelligence; memory; sex; sleep; sleep spindles

Introduction

Sleep spindles are typical features of nonrapid eye movement (NREM) sleep, arising as an interaction of thalamocortical, corticothalamic, and reticular neurons due to the absence of cholinergic activation during NREM sleep (Steriade and Deschenes, 1984; Amzica and Steriade, 2000; Steriade, 2000; Fogel and Smith, 2011). These oscillations provide excellent conditions for long-term synaptic changes (Buzsáki, 1989; Rosanova and Ulrich, 2005; Fogel and Smith, 2011), and the interplay of spindles and hippocampal ripples plays an important role in neuroplasticity (Clemens et al., 2007; Genzel et al., 2014). Specifically, spindles deafferent the cortex from the hippocampus, enabling local processing of increased firing rates in the cortex in response to hippocampal firing during ripples (Peyrache et al., 2009; Wierzynski et al., 2009; Genzel et al., 2014). Spindle activity indeed

correlates with memory consolidation in both declarative (Gais et al., 2002; Clemens et al., 2005; Genzel et al., 2009) and procedural (Fogel and Smith, 2006; Fogel et al., 2007; Morin et al., 2008) tasks.

Sleep spindles also reflect trait variables of cognition. Spindle parameters show strong intraindividual stability and are important components of the individual sleep EEG fingerprint (De Gennaro et al., 2005). Individual profiles in spindling reflect the microstructural properties of white matter tracts as measured by diffusion weighted MRI, with high levels of spindling being related to high axial diffusivity in white matter structures (Piantoni et al., 2013). Sleep spindle density correlates with measures of verbal memory (Lafortune et al., 2014), visuospatial memory (Bódizs et al., 2008), selective attention (Forest et al., 2007; Limoges et al., 2013), and fluid intelligence (Bódizs et al., 2005). Intelligence also correlates with the absolute number of spindles (Fogel et al., 2007), and sleep spindle duration and amplitude (Schabus et al., 2006; Fogel et al., 2007), suggesting that the efficiency of thalamocortical tracts reflected by prominent spindle activity is essential for overall cognitive ability.

However, previous studies were performed on relatively small and homogeneous samples (mainly university students of average to moderately high intelligence), rendering interpretation of correlation strength difficult. It is also unclear whether correlates of intelligence are similar throughout the entire IQ range (Fogel

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and Smith, 2011) and whether intelligence continues to correlate with spindle parameters within the extreme range, as correlates of intelligence often decrease with the distance from the average, a phenomenon known as the law of diminishing returns (Spearman, 1927; Tucker-Drob, 2009). Moreover, increased spindle activity has been reported not only in high IQ subjects, but also in children with mental retardation (Gibbs and Gibbs, 1962; Bixler and Rhodes, 1968); and, based on these findings, a U-shaped association between intelligence and sleep spindle activity has been proposed (Fogel et al., 2007; Fogel and Smith, 2011).

Sex differences were reported for the number of sleep spindles, spindle density, and EEG σ power (Gaillard and Blois, 1981; Carrier et al., 2001; Huupponen et al., 2002; Genzel et al., 2012) as well as functional correlates of spindles, namely, learning-related increases in spindle activity, which was only present in males and females in their mid-luteal menstrual phase (Genzel et al., 2012). Sex differences were also repeatedly shown for brain structures and neural correlates of cognitive performance (Cahill, 2006; Jazin and Cahill, 2010). Females generally show stronger values in various connectivity measures (Gong et al., 2009; Tomasi and Volkow, 2012; Ingahlhalikar et al., 2014; Satterthwaite et al., 2014) and stronger association between white matter and intellectual performance than males (Gur et al., 1999; Haier et al., 2005). We therefore hypothesized that the sleep spindle–IQ relationship is characterized by sexually dimorphic aspects, with females showing stronger correlations between intelligence and spindle activity than males.

Materials and Methods

We investigated the relationship between sleep spindle parameters and performance in tests of fluid reasoning, controlling for the effects of age and sex in a large sample. A total of 160 subjects (72 females, 88 males) participated in this study, in a cooperation between the Max Planck Institute of Psychiatry (Munich, Germany) and the Psychophysiology and Chronobiology Research Group of Semmelweis University (Budapest, Hungary). Mean age of subjects was 29.7 years (SD 10.7 years, range 17–69 years). The sleep spindle database was created using previously existing polysomnography recordings with available IQ scores, which has never been used in publications addressing the relationship between sleep spindles and intelligence, either in its entirety or in part. We further added new recordings specifically to increase the IQ variability within the sample, as our aim was to include subjects from a broad intelligence range. To avoid a masking of potential correlations between spindle parameters and intelligence through the inclusion of subjects with potentially pathological processes, we aimed to widen the intelligence distribution of our sample toward the upper extreme of the IQ range. We therefore recruited a considerable number of subjects among the members of the high-IQ society Mensa. The overall distribution of IQ scores is illustrated by Figure 1.

The research protocols were approved by the Ethical Committee of the Semmelweis University (Budapest, Hungary) or the Medical Faculty of the Ludwig Maximilians University (Munich, Germany) in accordance with the Declaration of Helsinki. All subjects signed informed consent for the participation in the studies. According to semistructured interview with experienced psychiatrists or psychologists, all subjects were healthy, had no history of neurologic or psychiatric disease, and were free of any current drug effects, excluding contraceptives. Consumption of small habitual doses of caffeine (maximum 2 cups of coffee before noon), but no alcohol, was allowed. Six male and 2 female subjects were light to moderate smokers (self-reported), and the rest of the subjects were nonsmokers.

Based on their availability, all subjects completed one or two standardized nonverbal intelligence tests. The tests used in the study were the Culture Fair Test (CFT) (Weiss and Weiss, 2006) and Raven Advanced Progressive Matrices (Raven APM, (Raven et al., 2004). Both the CFT and Raven APM are nonverbal intelligence tests where subjects are re-

quired to complete abstract patterns by finding their organizing rules. Performance in these tests was shown to correlate strongly and to be a particularly good measurement of the general factor of intelligence (Cattell, 1973; Duncan et al., 2000; Prokosh et al., 2005). A total of 113 subjects completed the CFT and 89 subjects completed the Raven APM test; 42 subjects completed both tests.

Sleep spindle parameters were expected to change as a factor of age, and IQ scores derived from intelligence tests are age-corrected, whereas raw scores of different intelligence tests are on different scales. Therefore, a composite raw intelligence test score was calculated, expressed as a Raven equivalent score. Raven equivalent scores for Raven APM tests were equal to the actual raw test score. For CFT raw scores, Raven equivalent scores were equal to the Raven APM score corresponding to the IQ percentile derived from CFT performance and the age of the subject, in other words, the Raven APM score that would have yielded the same population percentile score as the actually completed CFT test. If both Raven APM and CFT scores were available for a subject, the two Raven equivalent scores were averaged. Raven APM was chosen as a basis of standardization because of the availability of detailed norms. For this study, norms from the 1993 Des Moines (Iowa) standardization (Raven et al., 2004) of APM were used. Mean Raven equivalent score was 26.8 (SD 6.2, range 10.5–36). There was no difference in age ($F = 1.16$, $p > 0.9$) or Raven equivalent scores ($F = 1.36$, $p > 0.1$) between males (mean age 29.5 years, SD 10.4 years; mean Raven 27.5, SD 5.7) and females (mean age 29.3 years, SD 11.2 years; mean Raven 26.0, SD 6.7).

Sleep was recorded for two consecutive nights by standard polysomnography, including EEG according to the 10–20 system (Jaspers, 1958) (common recording sites across the studies and laboratories were as follows: Fp1, Fp2, F3, F4, Fz, F7, F8, C3, C4, Cz, P3, P4, T3, T4, T5, T6, O1, and O2), electro-oculography, bipolar submental electromyography, as well as electrocardiography. EEG electrodes were rereferenced to the mathematically linked mastoids. Impedances for the EEG electrodes were kept < 8 k Ω . Signals were collected, prefiltered, amplified, and digitized at different sampling rates using different recording apparatus in the different subsamples (Table 1).

Sleep EEG recordings for the second nights spent in the laboratory were manually scored on a 20 s basis by applying standard criteria (Iber, 2007). Epochs with artifacts were removed on a 4 s basis by visual inspection of all recorded channels (including polygraphy). The individual adjustment method (IAM) of sleep spindle analysis was applied for N2 and N3 sleep (Bódizs et al., 2009). The IAM procedure considers the individual spectral peaks as starting points for the sleep spindle analysis. In short, the second-order derivatives of 9–16 Hz amplitude spectra (4 s, Hanning tapered Fast Fourier Transform) of NREM sleep EEGs were averaged over EEG derivations and frequencies corresponding to the zero crossing points encompassing those two negative peaks with the largest absolute amplitudes were defined as frequency criteria for slow and fast sleep spindles. In cases of uncertainty (lack of zero crossing points indicating slow spindles or partial overlap between slow and fast sleep spindles in some cases), frequencies with predominance of power in averaged frontal (Fp1, Fp2, F3, F4, Fz, F7, F8) over averaged centroparietal (C3, C4, Cz, P3, P4) amplitude spectra were considered as slow spindle frequencies ($N = 18$). There was no case of uncertainty related to the frequency boundaries of fast spindles. Resulting slow and fast spindle boundaries were used as frequency limits for slow and fast spindle bandpass filtering (FFT-based, Gaussian filter, 16 s windows) of the EEGs.

Thresholding of the envelopes of the bandpass filtered EEGs were performed by using individual- and derivation-specific amplitude criteria: means of the amplitude spectral values (μV) at the frequencies corresponding to the lower and upper limits of sleep spindling were considered after multiplying by the number of bins making up the band. The envelope of the bandpass filtered signal had to exceed the threshold for at least 0.5 s to be considered a sleep spindle. Slow and fast sleep spindles defined in this way were counted and characterized by the following sleep spindle parameters:

1. Slow and fast sleep spindle density (spindles/minutes of N2 or N3 sleep, spindles min^{-1});

Table 1. Details of the recording procedures in different subsamples

	<i>N</i>	EEG recording sites (10–20 system)	Polygraphic channels	Electrodes used	Effective sampling rate/ sampling rate (Hz)
Budapest–I	31	Fp1, Fp2, F3, F4, Fz, F7, F8, C3, C4, Cz, P3, P4, T3, T4, T5, T6, O1, O2	Left and right EOG, bipolar submental EMG, ECG, thoracic and abdominal respiration	Au coated Ag/AgCl fixed with EC2 Grass electrode cream	249/249
Budapest–II	16	Fp1, Fp2, F3, F4, Fz, F7, F8, C3, C4, Cz, P3, P4, Pz, T3, T4, T5, T6, O1, O2	Bipolar EOG, bipolar submental EMG, ECG	Au coated Ag/AgCl fixed with EC2 Grass electrode cream	4096/1024
Munich–I	93	Fp1, Fp2, Fp3, AF1, AF2, F3, F4, Fz, F7, F8, C3, C4, Cz, P3, P4, Pz, T3, T4, T5, T6, O1, O2	Bipolar EOG, bipolar submental EMG, ECG	Ag/Ag–Cl, with EC2 Grass electrode cream for EEG and Nihon Kohden ELEFIX for EMG	250/250
Munich–II	20	Fp1, Fp2, F3, F4, C3, C4, P3, P4, O1, O2	Bipolar EOG, bipolar submental EMG, ECG	Ag/Ag–Cl, with EC2 Grass electrode cream for EEG and Nihon Kohden ELEFIX for EMG	250/250

2. Slow and fast sleep spindle durations (mean duration of sleep spindles detected, seconds);
3. Slow and fast sleep spindle amplitudes (mean maxima of the intraspindle envelopes of bandpass filtered EEGs, μV);
4. The peak frequencies and upper/lower frequency limits of slow and fast spindles for each subject.

To correct for the different analog EEG filter characteristics of our machines, we connected an analog waveform generator to the C3 and C4 electrode inputs (with original recording reference, rereferenced for A1–A2 common references for further analysis) of all EEG devices and applied 40 and 355 μV amplitude sinusoid signals of various amplitudes (0.05 Hz, every 0.1 Hz between 0.1–2 Hz, every 1 Hz between 2–20 Hz, every 10 Hz between 10 Hz–100 Hz).

We determined the amplitude reduction rate of each recording system by calculating the proportion between digital (measured) and analog (generated) amplitudes of sinusoid signals at typical sleep spindle frequencies (10, 11, 12, 13, 14, and 15 Hz) for both inducing (40 and 355 μV amplitude) signals. Machine-specific amplitude reduction rates were given as the mean amplitude rate between digital and analog values at the two amplitudes and six measured frequencies (for the reduction rates, see Table 1). Sleep spindle amplitudes were corrected by dividing their calculated values by the amplitude reduction rate of the recording system.

Given the individual- and derivation-specific adjustment inherent to the procedure, sleep spindle densities and durations are amplitude-insensitive measures (for an empirical demonstration, see Bódizs et al., 2005). Thus, there is no need for the compensation of the different recording systems in these values. Group comparisons (male vs female) were performed by independent samples *t* tests. Partial Pearson correlation coefficients were calculated to test the relationship between sleep spindle parameters and Raven equivalent scores, controlling for the effects of age. This was deemed necessary because of the potential effects of age on both sleep spindle parameters (De Gennaro and Ferrara, 2003; Fogel and Smith, 2011) and intelligence test performance (Tucker-Drob, 2009). To control for multiple comparisons across electrodes, we performed the Benjamini–Hochberg procedure (Benjamini and Hochberg, 1995) controlling for the false discovery rate for each sleep spindle parameter. This correction procedure was selected because sleep spindle parameters at different electrodes are expected to correlate positively, rendering a Bonferroni correction overly conservative. The Benjamini–Hochberg procedure, on the other hand, is valid for both independent and positively correlated tests.

To allow for a better comparison with previous studies, the correlations that were strongest using the IAM method were recalculated with spindle measures using a fixed-criterion spindle detection algorithm as common in related research (e.g., Schabus et al., 2007) with fixed threshold frequencies 11–13 Hz for slow spindles and 13–15 Hz for fast spindles. Of note, a fixed-criterion method is inherently less sensitive than IAM because it does not take into account individual variations in sleep spindle frequency, instead analyzing a relatively broad frequency band. It is also noteworthy that the fixed-criterion method used somewhat arbitrary detection frequencies, classifying anything < 13 Hz as a slow spindle and completely missing sleep spindles slower than 11 Hz. This might lead to incorrect classification of spindles in some subjects as well as missed detections of the slowest spindles. However, fast spindle amplitude on a

prominent fast-spindle generating site (Cz) is a feature salient enough to be reliably detected even with a less sensitive spindle detection method.

Results

In general, slow spindle amplitude was highest at frontal derivations (maximum amplitude on Fz), whereas fast spindles were most prominent on central and parietal derivations (maximum amplitude on Cz). Mean peak frequency was 11.43 Hz (SD 0.76 Hz, range 9.59–13.28 Hz) for slow spindles and 13.72 Hz (SD 0.59 Hz, range 12.5–15.38 Hz) for fast spindles.

Age was in significant negative correlation with all sleep spindle parameters on all electrodes, except for slow spindle amplitude on all electrodes, slow spindle duration on Cz, Fz, and T5, and fast spindle amplitude on O1 and O2. Positive correlations between age and slow spindle amplitude were significant on O2 (median amplitude only) and P4 (both median and maximum amplitude). A significant positive correlation with fast spindle peak frequency and significant negative correlation with Raven equivalent raw scores was also found.

Sex differences were found in various sleep spindle parameters. Women had significantly higher fast spindle amplitudes in derivations F3, F4, Fz, C3, C4, Cz, P3, P4, T6, O1, and O2, and higher peak frequencies both in case of slow and fast spindles. Men had significantly higher fast spindle densities on derivations P3, P4, O1, and O2, and significantly higher fast spindle durations on O2.

Sex differences were found in various sleep spindle parameters. Women had significantly higher fast spindle amplitudes in derivations F3 (Mean_{male} = 4.61, Mean_{female} = 5.13, $t = -2.18$, $p = 0.03$), F4 (Mean_{male} = 4.66, Mean_{female} = 5.3, $t = -2.66$, $p = 0.008$), Fz (Mean_{male} = 5.29, Mean_{female} = 5.99, $t = -2.39$, $p = 0.02$), C3 (Mean_{male} = 5.20, Mean_{female} = 5.82, $t = -2.55$, $p = 0.01$), C4 (Mean_{male} = 5.24, Mean_{female} = 4.92, $t = -2.83$, $p = 0.005$), Cz (Mean_{male} = 6.81, Mean_{female} = 8.02, $t = -3.55$, $p = 0.0005$), P3 (Mean_{male} = 5.43, Mean_{female} = 6.2, $t = -2.99$, $p = 0.003$), P4 (Mean_{male} = 5.22, Mean_{female} = 5.91, $t = -2.66$, $p = 0.009$), T6 (Mean_{male} = 2.97, Mean_{female} = 3.28, $t = -2.07$, $p = 0.04$), O1 (Mean_{male} = 3.81, Mean_{female} = 4.36, $t = -2.51$, $p = 0.01$), and O2 (Mean_{male} = 3.77, Mean_{female} = 4.22, $t = -2.14$, $p = 0.03$), and higher peak frequencies (Hz) in case of both slow (Mean_{male} = 11.28, Mean_{female} = 11.61, $t = -2.82$, $p = 0.005$) and fast (Mean_{male} = 13.55, Mean_{female} = 13.92, $t = -4.13$, $p = 0.00006$) spindles. Men had significantly higher fast spindle densities (no./min) on derivations P3 (Mean_{male} = 7.64, Mean_{female} = 7.34, $t = 2.00$, $p = 0.04$), P4 (Mean_{male} = 7.60, Mean_{female} = 7.30, $t = 2.00$, $p = 0.04$), O1 (Mean_{male} = 7.24, Mean_{female} = 6.84, $t = 2.35$, $p = 0.02$), and O2 (Mean_{male} = 7.29, Mean_{female} = 6.76, $t = 3.08$, $p = 0.002$), and significantly higher fast spindle durations on O2 (Mean_{male} = 1.09, Mean_{female} = 1.03, $t = 2.57$, $p = 0.01$).

Strong sex differences were found in correlations between sleep spindle parameters and Raven equivalent scores. In females,

Table 1. Continued

	Precision	Hardware prefiltering (Hz)	Amplitude attenuation 10–15 Hz (mean [SD])	Recording apparatus	Recording software
Budapest–I	12bit	0.5–70	0.9705 [0.0036]	Flat Style SLEEP La Mont Headbox, HBX32-SLP preamplifier (La Mont Medical)	DataLab (Medcare)
Budapest–II	12bit	0.33–1500 (<450 Hz antialiasing digital filtering before undersampling)	0.9356 [0.0021]	Brain-Quick BQ 1325 (Micromed)	System 98 (Micromed)
Munich–I	8bit	0.53–70	0.9693 [0.0016]	Comlab 32 DigitalSleep Lab	Brainlab, version 3.3
Munich–II	8bit	0.53–70	0.9693 [0.0016]	Comlab 32 DigitalSleep Lab	Brainlab, version 3.3

Table 2. Partial Pearson correlation coefficients (corrected for age) between sleep spindle parameters and Raven APM scores in female subjects^a

		Slow spindles								Fast spindles							
		Density		Duration		Median amplitude		Maximum amplitude		Density		Duration		Median amplitude		Maximum amplitude	
	<i>N</i>	<i>df</i>	<i>R</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>p</i>
Fp1	72	69	0.273	0.036	0.271	0.038	−0.075	0.570	−0.081	0.540	0.114	0.391	0.056	0.672	0.285	0.029	0.292
Fp2	72	69	0.291	0.026	0.262	0.045	−0.086	0.516	−0.094	0.480	0.140	0.290	0.089	0.505	0.265	0.042	0.267
Fz	60	57	0.286	0.028	0.338*	0.009	−0.187	0.156	−0.188	0.155	0.089	0.503	0.050	0.709	0.334	0.010	0.335*
F3	72	69	0.265	0.042	0.260	0.047	−0.076	0.568	−0.083	0.533	0.107	0.421	0.101	0.447	0.274	0.036	0.277
F4	72	69	0.261	0.046	0.262	0.045	−0.102	0.441	−0.108	0.417	0.127	0.336	0.120	0.364	0.277	0.034	0.281
F7	60	57	0.328	0.011	0.368*	0.004	−0.162	0.220	−0.166	0.208	−0.012	0.930	−0.019	0.889	0.183	0.167	0.185
F8	60	57	0.328	0.011	0.374*	0.004	−0.165	0.213	−0.167	0.207	0.059	0.656	0.015	0.910	0.234	0.075	0.231
C3	72	69	0.247	0.060	0.254	0.052	−0.110	0.408	−0.117	0.379	0.082	0.537	0.133	0.316	0.365	0.004	0.367*
C4	72	69	0.259	0.047	0.259	0.048	−0.131	0.324	−0.135	0.308	0.134	0.310	0.130	0.327	0.371	0.004	0.371*
Cz	60	57	0.295	0.023	0.356*	0.006	−0.194	0.142	−0.194	0.142	0.083	0.533	0.092	0.488	0.412	0.001	0.410*
P3	72	69	0.231	0.078	0.268	0.040	−0.148	0.264	−0.150	0.256	0.036	0.788	0.135	0.308	0.281	0.031	0.283
P4	72	69	0.241	0.066	0.270	0.039	−0.136	0.305	−0.140	0.290	0.084	0.528	0.126	0.340	0.282	0.030	0.284
T3	60	57	0.314	0.015	0.379*	0.003	−0.172	0.193	−0.176	0.183	0.027	0.837	0.019	0.887	0.210	0.110	0.203
T4	60	57	0.306	0.018	0.374*	0.004	−0.214	0.104	−0.214	0.104	−0.017	0.898	−0.010	0.940	0.030	0.819	0.027
T5	60	57	0.288	0.027	0.372*	0.004	−0.226	0.085	−0.223	0.089	−0.019	0.886	0.070	0.598	0.152	0.251	0.154
T6	60	57	0.312	0.016	0.363*	0.005	−0.282	0.030	−0.278	0.033	0.033	0.806	0.045	0.737	0.059	0.656	0.064
O1	72	69	0.258	0.049	0.263	0.045	−0.173	0.191	−0.173	0.189	0.027	0.841	0.116	0.380	0.158	0.233	0.160
O2	72	69	0.273	0.036	0.261	0.046	−0.190	0.149	−0.194	0.141	0.089	0.503	0.122	0.359	0.129	0.330	0.133

^aIn the first two columns, the number of available subjects and the corresponding degrees of freedom are given for each electrode.

*Correlations that remain significant after multiple comparisons correction.

age-corrected partial correlations were significant between Raven equivalent scores and fast spindle amplitude (central, frontal, and parietal derivations, $r_{\max} = 0.412$ on Cz) and slow spindle duration (all derivations with the exception of C3, $r_{\max} = 0.379$ on T3). In males, age-corrected partial correlations revealed a negative association between Raven equivalent scores and fast spindle density (posterior derivations, $r_{\max} = -0.337$ on O1). After correction for multiple testing, partial correlation coefficients were significant between Raven equivalent scores and fast spindle amplitude (electrodes Cz, C3, C4, and Fz) and slow spindle duration (electrodes F7, F8, T3, T4, T5, T6, Cz, and Fz) in females, as well as fast spindle density (electrodes O1, O2, P3, P4, and T5) in males.

Table 2 gives an overview of the partial correlations found in females. Table 3 gives an overview of the partial correlations found in males. Table 4 gives an overview of partial correlations in all subjects. Figure 1 illustrates the most prominent partial correlations between Raven equivalent scores, fast spindle amplitude, slow spindle duration, and fast spindle density in both sexes.

Sex differences in the correlations between Raven equivalent scores and sleep spindle parameters were confirmed by statistical comparison of the maximal significant correlations illustrated in Figure 2. Using Fisher's r to z transformation method, correlation

coefficients found in males and females were significantly different for fast spindle amplitude on Cz ($z = 3.2$, $p = 0.001$), slow spindle duration on T3 ($z = 3.23$, $p = 0.001$), and fast spindle density on O1 ($z = 2.23$, $p = 0.02$).

Sleep spindle peak frequencies were not correlated with Raven equivalent scores in either sex and in either slow or fast spindles (age-corrected partial correlation with slow spindle peak frequency is 0.17 [$p = 0.160$] in females, -0.06 [$p = 0.539$] in males; correlation with fast spindle peak frequency is -0.04 [$p = 0.744$] in females, 0.095 [$p = 0.379$] in males).

Similar results were seen if individual intelligence test raw scores (CFT or Raven) were used instead of the combined score. Correlations were also not exclusively driven by either subgroup (Budapest or Munich) used in the study (for details, see Fig. 2, scatterplots). Inclusion or exclusion of the 8 smoking subjects did not change the results of the study.

To replicate our main findings with 90% statistical power, a sample size of $n = 48$ would be required for fast spindle amplitude on Cz ($r = 0.41$), a sample size of $n = 56$ would be required for slow spindle duration on T3 ($r = 0.371$), and a sample size of $n = 72$ would be required for fast spindle density on O1 ($r = -0.337$). Given that these sample sizes are meant for subjects from the same sex due to sex differences in the relationship

Table 3. Partial Pearson correlation coefficients (corrected for age) between sleep spindle parameters and Raven APM scores in male subjects^a

	<i>N</i>	<i>df</i>	Slow spindles								Fast spindles							
			Density		Duration		Median amplitude		Maximum amplitude		Density		Duration		Median amplitude		Maximum amplitude	
			<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>
Fp1	88	85	−0.016	0.890	−0.100	0.379	−0.102	0.370	−0.101	0.374	−0.182	0.106	−0.123	0.278	−0.173	0.126	−0.177	0.117
Fp2	88	85	0.005	0.963	−0.102	0.366	−0.087	0.442	−0.077	0.500	−0.168	0.135	−0.090	0.429	−0.172	0.128	−0.165	0.145
Fz	81	78	0.045	0.690	−0.080	0.481	−0.038	0.741	−0.030	0.791	−0.241	0.032	−0.086	0.450	−0.110	0.330	−0.109	0.337
F3	88	85	0.043	0.707	−0.083	0.466	−0.065	0.565	−0.057	0.617	−0.241	0.031	−0.107	0.345	−0.124	0.274	−0.125	0.271
F4	88	85	0.012	0.917	−0.095	0.401	−0.078	0.493	−0.068	0.552	−0.211	0.060	−0.041	0.719	−0.136	0.228	−0.134	0.236
F7	81	78	0.045	0.694	−0.094	0.405	−0.036	0.754	−0.030	0.792	−0.172	0.128	−0.073	0.520	−0.093	0.413	−0.087	0.445
F8	81	78	0.027	0.815	−0.108	0.341	−0.078	0.492	−0.071	0.530	−0.167	0.139	−0.027	0.816	−0.145	0.199	−0.134	0.237
C3	88	85	0.096	0.395	−0.099	0.384	−0.073	0.518	−0.065	0.568	−0.238	0.033	−0.127	0.262	−0.114	0.316	−0.110	0.331
C4	88	85	0.064	0.573	−0.109	0.335	−0.093	0.411	−0.083	0.462	−0.219	0.051	−0.084	0.460	−0.128	0.259	−0.124	0.273
Cz	81	78	0.094	0.407	−0.106	0.350	−0.055	0.629	−0.050	0.661	−0.234	0.037	−0.090	0.426	−0.081	0.476	−0.079	0.489
P3	88	85	0.098	0.388	−0.135	0.232	−0.111	0.325	−0.102	0.367	−0.309*	0.005	−0.121	0.286	−0.189	0.093	−0.184	0.103
P4	88	85	0.122	0.282	−0.118	0.296	−0.059	0.602	−0.051	0.656	−0.312*	0.005	−0.128	0.260	−0.138	0.222	−0.134	0.236
T3	81	78	0.085	0.456	−0.124	0.272	−0.117	0.301	−0.117	0.302	−0.165	0.144	−0.066	0.563	−0.190	0.092	−0.182	0.107
T4	81	78	0.062	0.584	−0.121	0.285	−0.134	0.235	−0.125	0.271	−0.162	0.150	−0.055	0.626	−0.197	0.080	−0.163	0.148
T5	81	78	0.097	0.391	−0.132	0.244	−0.069	0.542	−0.065	0.565	−0.287*	0.010	−0.108	0.340	−0.063	0.577	−0.059	0.604
T6	81	78	0.074	0.512	−0.134	0.235	−0.121	0.286	−0.113	0.317	−0.266	0.017	−0.089	0.432	−0.144	0.204	−0.140	0.214
O1	88	85	0.083	0.462	−0.140	0.216	−0.081	0.477	−0.071	0.531	−0.337*	0.002	−0.140	0.216	−0.128	0.256	−0.125	0.268
O2	88	85	0.104	0.357	−0.126	0.265	−0.066	0.559	−0.054	0.634	−0.315*	0.004	−0.128	0.259	−0.143	0.207	−0.139	0.219

^aIn the first two columns, the number of available subjects and the corresponding degrees of freedom are given for each electrode.

*Correlations that remain significant after multiple comparisons correction.

Table 4. Partial Pearson correlation coefficients (corrected for age) between sleep spindle parameters and Raven APM scores in all subjects^a

	<i>N</i>	<i>df</i>	Slow spindles								Fast spindles							
			Density		Duration		Median amplitude		Maximum amplitude		Density		Duration		Median amplitude		Maximum amplitude	
			<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>	<i>r</i>	<i>p</i>
Fp1	160	157	0.127	0.135	0.073	0.393	−0.083	0.327	−0.085	0.321	−0.039	0.650	−0.025	0.769	0.038	0.659	0.035	0.685
Fp2	160	157	0.144	0.089	0.066	0.441	−0.082	0.338	−0.079	0.354	−0.025	0.769	0.007	0.935	0.021	0.806	0.023	0.791
Fz	141	138	0.156	0.066	0.076	0.371	−0.075	0.381	−0.074	0.388	−0.071	0.406	0.007	0.937	0.052	0.544	0.053	0.535
F3	160	157	0.136	0.109	0.070	0.409	−0.096	0.257	−0.094	0.270	−0.049	0.567	0.050	0.561	0.038	0.652	0.040	0.636
F4	160	157	0.183	0.031	0.112	0.188	−0.107	0.207	−0.106	0.214	−0.100	0.242	−0.035	0.681	0.021	0.804	0.024	0.776
F7	141	138	0.168	0.047	0.106	0.211	−0.129	0.129	−0.126	0.137	−0.077	0.365	−0.001	0.995	0.011	0.902	0.015	0.861
F8	141	138	0.167	0.049	0.111	0.193	−0.127	0.135	−0.123	0.147	−0.084	0.327	−0.011	0.895	0.068	0.424	0.069	0.415
C3	160	157	0.173	0.041	0.064	0.452	−0.103	0.225	−0.102	0.229	−0.071	0.406	0.011	0.902	0.082	0.339	0.083	0.328
C4	160	157	0.160	0.059	0.060	0.481	−0.121	0.156	−0.118	0.165	−0.042	0.626	0.034	0.690	0.076	0.372	0.078	0.359
Cz	141	138	0.198	0.019	0.103	0.224	−0.143	0.093	−0.140	0.099	−0.078	0.360	0.005	0.954	0.094	0.269	0.095	0.264
P3	160	157	0.168	0.047	0.052	0.542	−0.141	0.098	−0.137	0.108	−0.111	0.190	0.021	0.804	0.010	0.907	0.015	0.864
P4	160	157	0.182	0.032	0.058	0.493	−0.111	0.191	−0.109	0.199	−0.093	0.277	0.014	0.868	0.034	0.687	0.037	0.661
T3	141	138	0.200	0.018	0.098	0.252	−0.154	0.070	−0.155	0.068	−0.064	0.453	−0.017	0.842	−0.035	0.678	−0.035	0.686
T4	141	138	0.179	0.035	0.096	0.261	−0.179	0.034	−0.174	0.040	−0.104	0.222	−0.030	0.725	−0.104	0.221	−0.090	0.292
T5	141	138	0.198	0.019	0.089	0.295	−0.171	0.044	−0.167	0.049	−0.127	0.134	−0.006	0.943	−0.003	0.974	−0.001	0.996
T6	141	138	0.192	0.023	0.083	0.329	−0.224	0.008	−0.219	0.009	−0.107	0.206	−0.011	0.902	−0.087	0.307	−0.083	0.328
O1	160	157	0.170	0.044	0.044	0.603	−0.145	0.087	−0.140	0.099	−0.122	0.152	0.004	0.964	−0.022	0.797	−0.020	0.814
O2	160	157	0.184	0.030	0.051	0.551	−0.147	0.083	−0.142	0.095	−0.062	0.468	0.017	0.839	−0.036	0.671	−0.033	0.697

^aIn the first two columns, the number of available subjects and the corresponding degrees of freedom are given for each electrode. No correlations are significant after multiple comparisons correction.

between IQ and spindles, previous studies appear to have been underpowered.

The correlations that were strongest using the IAM method were recalculated with sleep spindle parameters calculated by a fixed amplitude detection method. In this method, we filtered data for the individual IAM frequencies and applied a fixed amplitude threshold set at 4 μ V for slow spindles and 6 μ V for fast spindles. These amplitude criteria were defined based on the 12 μ V amplitude limit of the Somnolyzer SIESTA fixed amplitude spindle detection method (Anderer et al., 2005) but reduced because of the narrower frequency bands used in IAM. The amplitude criteria were kept intentionally high to reduce false-positive

detections in subjects with high baseline EEG voltage: therefore, depending on the electrode, 1–8 female and 2–12 male subjects provided zero detections and were not considered for the analysis of spindle parameters on the given electrode.

Data from this alternative approach successfully replicated our main finding: the age-corrected partial correlation between intelligence and fast spindle median amplitude on Cz was significant after correction for multiple testing in females ($N = 71$, $r = 0.41$, $p = 0.001$), but not in males ($N = 79$, $r = 0.005$, $p = 0.965$). Furthermore, we found a significant positive correlation between intelligence and fast spindle density on C4, Cz, and Fz in females ($N = 71$ for C4, $N = 59$ for Cz and Fz, $r_{\max} = 0.373$ on Cz, $p =$

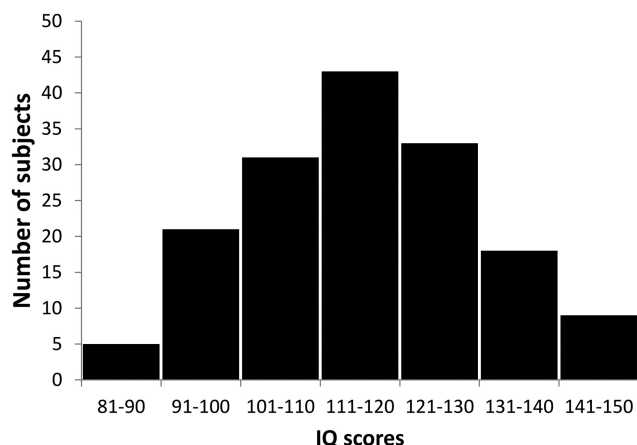


Figure 1. Distribution of IQ scores in the sample.

0.004) as well as a positive correlation between intelligence and fast spindle duration on O1 and O2 in males ($N = 81$, $r_{\max} = 0.356$ on O2, $p = 0.002$). Other spindle parameters did not correlate significantly with intelligence scores after multiple testing correction in either sex.

Discussion

Different sleep spindle parameters have repeatedly been associated with state and trait measures of cognitive variables (Fogel and Smith, 2011). However, typical study samples consisted of a rather small number of university students, leading to results that rely on a restricted variance in intelligence scores. Testing the stability of the correlates of intelligence over the entire intelligence range requires the inclusion of a relatively high number of subjects representing also the extremes of the IQ distribution. In our study, we analyzed data of 160 subjects, including many subjects with high and very high intelligence scores. Our findings did not indicate decreasingly linear associations within the extreme IQ ranges, suggesting that the functional and physiological significance of sleep spindles is consistent across the entire intelligence distribution. In contrast to the proposed U-shaped association between intelligence and sleep spindle activity (Fogel et al., 2007; Fogel and Smith, 2011), we found this association to be linear.

In line with previous research (Principe and Smith, 1982; Dijk et al., 1989; Landolt et al., 1996; Carrier et al., 2001; Nicolas et al., 2001; Bódizs et al., 2009), our study revealed a generally negative correlation between age and most measures of sleep spindle activity, and a positive correlation between age and spindle frequency. Slow spindles appeared to be less affected by aging, as for these we found no negative correlation with amplitude (indeed, there was a positive correlation on O2 and P4, which however did not survive correction for multiple comparisons) and on some electrodes (Cz, Fz, T5) no negative correlation with duration either. This suggests that, whereas slow spindle density and (in most cases) duration decrease with age, amplitude is preserved, supporting previous evidence about different neural mechanisms being involved in slow and fast spindles (Schabus et al., 2007). The absence of correlations with fast spindle amplitudes at occipital derivations probably stems from an already low level of spindle activity on these non-prominent spindle locations in a younger age.

Previous research has never specifically looked for sex differences in the sleep EEG correlates of intelligence. However, striking sex differences are known not only for brain anatomy in general (Cahill, 2006; Gong et al., 2009; Jazin and Cahill, 2010;

Tomasi and Volkow, 2012; Ingallhalikar et al., 2014; Satterthwaite et al., 2014) and sleep spindle activity (Huupponen et al., 2002), but specifically for neural correlates of intelligence as measured by waking EEG (Neubauer et al., 2002; Jausovec and Jausovec, 2005) or brain anatomy (Gur et al., 1999; Haier et al., 2005). In addition, sleep spindle activity differentially affects memory consolidation in males and females (Genzel et al., 2012). Most notably, white matter microstructure was shown to be closely associated with sleep spindle activity (Piantoni et al., 2013) and intelligence in females, but not in males (Gur et al., 1999; Haier et al., 2005). In line with these observations, our analyses revealed marked sex differences in the association between intelligence and sleep spindle activity: we found a correlation between Raven equivalent scores and fast sleep spindle amplitudes in central derivations in females, but not in males. Our findings suggest that thalamocortical connections underlying EEG sleep spindle activity are associated with intelligence in females, but not in males.

The positive association between Raven equivalent scores and slow spindle durations was generally present at almost all scalp locations, most prominent in temporal derivations, and found exclusively in females. Sleep spindles coalesce with cortical slow oscillations (Steriade, 2003), and the strength of this temporal synchrony between slow oscillation up-states and sleep spindles was shown to be positively correlated with intellectual performance (Bódizs et al., 2005). A positive relationship between slow-wave upstate length and memory consolidation has also been demonstrated (Heib et al., 2013). Based on these findings, our results suggest that longer slow sleep spindle durations in more intelligent females might reflect more precise coalescence between sleep spindles and cortical slow oscillations or easier elicibility of spindles by such oscillations.

The correlation between intelligence and slow spindle duration was maximal in temporal derivations. Regional sleep spindles at a certain cortical location are not necessarily byproducts of sleep spindles at more prominent locations but arise from the activity of local corticothalamic oscillations (Nir et al., 2011), and localized sleep spindles play a role in local synaptic plasticity and subsequent sleep-related learning (Nishida and Walker, 2007). Generally, strong neural activation increases related to slow spindles have been demonstrated for the temporal lobe (Schabus et al., 2007). The lateral frontal and temporal maximum of our findings likely has functional importance, suggesting that, in females, longer sleep spindle durations are connected to intelligence mainly in cortical areas responsible for higher-order visual processing and language. Interestingly, structural imaging studies have found a positive correlation between intelligence in females and white matter volume in Broca's area (Haier et al., 2005), an overlapping and at least in part functionally similar (language-related) brain region.

In males, a negative association between Raven equivalent scores and fast spindle density was found, limited to posterior scalp locations with a left occipital maximum. This finding conflicts with earlier research with samples, including both males and females (Fogel and Smith, 2011), however, is in line with a study of male rats that found learning potential to be negatively associated with spindle density (Fogel et al., 2010). Based on the topography and locally limited nature of our findings, it might be speculated that lower occipital fast spindle density in highly intelligent males is due to higher neural efficiency of the lower-level visual areas. Of note, also in human waking EEG, evidence for higher neural efficiency being associated with intelligence was found in males only (Jausovec and Jausovec, 2005; Neubauer and Fink, 2009).

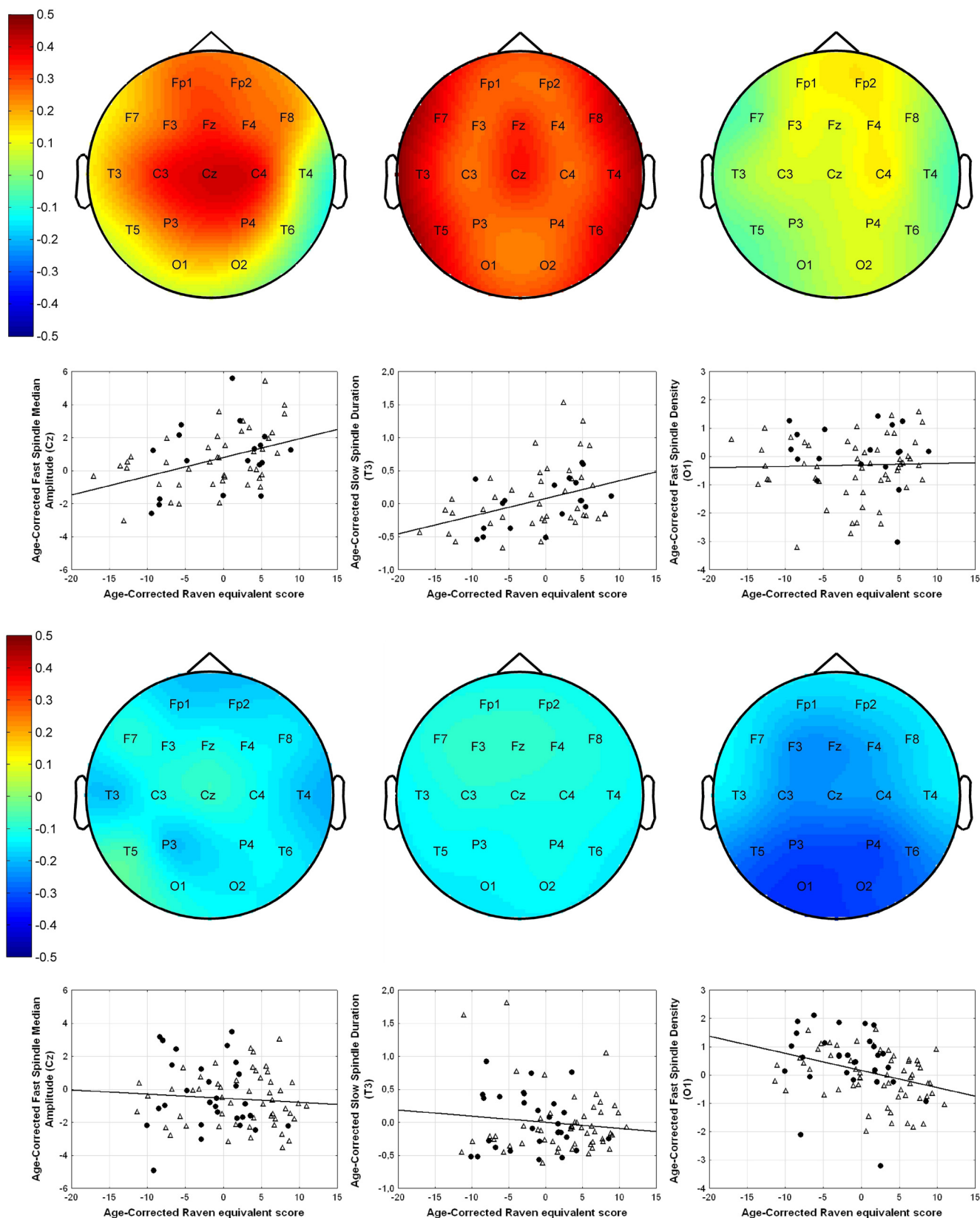


Figure 2. Scalp maps and partial regression plots for females (top half) and males (bottom half), for Cz fast spindle median amplitude (left), T3 slow spindle duration (middle), and O1 fast spindle density (right). Scalp maps illustrate the topographical distribution of the strength of partial correlations between Raven equivalent scores and sleep spindle parameters. On the partial regression plots, x-axes represent the residuals after regressing Raven APM scores against age. y-axes represent the residuals after regressing spindle parameters against age. Thus, these scatterplots demonstrate the relationship between Raven APM scores and spindle parameters after pruning both variables for the effects of age. Standard Pearson correlation between the shown residuals equals the age-corrected partial correlations between Raven APM scores and spindle parameters. Dots represent data points from the Budapest sample. Triangles represent data points from the Munich sample.

Table 5. Earlier studies reporting associations between sleep spindle parameters and intelligence^a

Reference	Test	Age	Sex	Spindle parameter	Electrode	Correlation
Bodizs et al., 2005	RPMT: IQ	27–67 years	5 f/14 m	Density slow	Fp1, Fp2, Fpz, F3, F4, Fz, F7, F8, C3, C4, Cz, T3, T4, T5, T6, P3, P4, Pz, O1, O2, Oz	NS
Bodizs et al., 2005	RPMT: IQ	27–67 years	5 f/14 m	Density fast	Fp1, Fp2, Fpz, F3, F4, Fz, F7, F8, C3, C4, Cz, T3, T4, T5, T6, P3, P4, Pz, O1, O2, Oz	From $r = 0.25, p = 0.33$ at O2 to $r = 0.79, p = 0.0001$ at Fp2
Clemens et al., 2006	RPMT: IQ	25–47 years, mean 35, SD 7.7	15 m	Total number	Fp1, Fpz, Fp2, F7, F3, Fz, F4, F8, T3, C3, Cz, C4, T4, T5, P3, Pz, P4, T6, O1, Oz, O2	NS
Schabus et al., 2006	APM: IQ	20–30 years, mean 24, SD 2.6	24 f/24 m	Activity slow	C3	$r = 0.40, p < 0.01$
Schabus et al., 2006	APM: IQ	20–30 years, mean 24, SD 2.6	24 f/24 m	Activity fast	C3	$r = 0.44, p < 0.01$
Schabus et al., 2006	APM: IQ	20–30 years, mean 24, SD 2.6	24 f/24 m	Density slow	C3	$r = 0.06, p = 0.68$
Schabus et al., 2006	APM: IQ	20–30 years, mean 24, SD 2.6	24 f/24 m	Density fast	C3	$r = -0.01, p = 0.97$
Schabus et al., 2006	APM: IQ	20–30 years, mean 24, SD 2.6	24 f/24 m	Duration slow	C3	$r = 0.09, p = 0.54$
Schabus et al., 2006	APM: IQ	20–30 years, mean 24, SD 2.6	24 f/24 m	Duration fast	C3	$r = 0.34, p = 0.02$
Schabus et al., 2006	APM: IQ	20–30 years, mean 24, SD 2.6	24 f/24 m	Amplitude slow	C3	$r = 0.39, p = 0.01$
Schabus et al., 2006	APM: IQ	20–30 years, mean 24, SD 2.6	24 f/24 m	Amplitude fast	C3	$r = 0.35, p = 0.02$
Fogel et al., 2007	MAB-II: VIQ	18–29 years	10 f	Total number	C3, C4	$r = 0.56, p = 0.09$
Fogel et al., 2007	MAB-II: PIQ	18–29 years	10 f	Total number	C3, C4	$r = 0.71, p = 0.02$
Fogel et al., 2007	MAB-II: FSIQ	18–29 years	10 f	Total number	C3, C4	$r = 0.76, p = 0.01$
Fogel et al., 2007	MAB-II: VIQ	20–25 years	12 f	Total number	C3, C4	$r = 0.38, p = 0.10$
Fogel et al., 2007	MAB-II: PIQ	20–25 years	12 f	Total number	C3, C4	$r = 0.79, p = 0.001$
Fogel et al., 2007	MAB-II: VIQ	20–25 years	12 f	Total number	Cz	$r = 0.01, p = 0.94$
Fogel et al., 2007	MAB-II: PIQ	20–25 years	12 f	Total number	Cz	$r = 0.05, p = 0.79$
Fogel et al., 2007	MAB-II: VIQ	18–26 years, mean 20, SD 5.3	29 f/6 m	Density	Cz	NS
Fogel et al., 2007	MAB-II: PIQ	18–26 years, mean 20, SD 5.3	29 f/6 m	Density	Cz	NS
Fogel et al., 2007	MAB-II: VIQ	18–26 years, mean 20, SD 5.3	29 f/6 m	Duration	Cz	NS
Fogel et al., 2007	MAB-II: PIQ	18–26 years, mean 20, SD 5.3	29 f/6 m	Duration	Cz	NS
Peters et al., 2007	MAB-II: VIQ	Mean 21, SD 2.4	12 f/12 m	Density	C3, C4	$r = -0.26, p > 0.05$
Peters et al., 2007	MAB-II: PIQ	Mean 21, SD 2.4	12 f/12 m	Density	C3, C4	$r = 0.05, p > 0.05$
Peters et al., 2007	MAB-II: FSIQ	Mean 21, SD 2.4	12 f/12 m	Density	C3, C4	$r = -0.11, p > 0.05$
Peters et al., 2008	MAB-II: VIQ	17–24 years, mean 20, SD 2.3	7 f/7 m	Density	C3, C4	NS
Peters et al., 2008	MAB-II: PIQ	17–24 years, mean 20, SD 2.3	7 f/7 m	Density	C3, C4	NS
Peters et al., 2008	MAB-II: FSIQ	17–24 years, mean 20, SD 2.3	7 f/7 m	Density	C3, C4	NS
Peters et al., 2008	MAB-II: VIQ	62–79 years, mean 70, SD 5.1	7 f/7 m	Density	C3, C4	NS
Peters et al., 2008	MAB-II: PIQ	62–79 years, mean 70, SD 5.1	7 f/7 m	Density	C3, C4	NS
Peters et al., 2008	MAB-II: FSIQ	62–79 years, mean 70, SD 5.1	7 f/7 m	Density	C3, C4	NS
Tucker and Fishbein, 2009	MAB-II: VIQ	Mean 21 years	12 f/12 m	Sigma power	C3, C4	NS
Tucker and Fishbein, 2009	MAB-II: PIQ	Mean 21 years	12 f/12 m	Sigma power	C3, C4	NS
Tucker and Fishbein, 2009	MAB-II: FSIQ	Mean 21 years	12 f/12 m	Sigma power	C3, C4	NS
Geiger et al., 2011	WISC-IV: VIQ	9–13 years, mean 10.5	6 f/8 m	Spindle peak frequency	C3, C4	NS
Geiger et al., 2011	WISC-IV: FIQ	9–13 years, mean 10.5	6 f/8 m	Spindle peak frequency	C3, C4	NS
Geiger et al., 2011	WISC-IV: FSIQ	9–13 years, mean 10.5	6 f/8 m	Spindle peak frequency	C3, C4	$r = -0.56, p < 0.05$
Geiger et al., 2011	WISC-IV: VIQ	9–13 years, mean 10.5	6 f/8 m	Sigma power	C3, C4	NS
Geiger et al., 2011	WISC-IV: FIQ	9–13 years, mean 10.5	6 f/8 m	Sigma power	C3, C4	$r = 0.65, p < 0.05$
Geiger et al., 2011	WISC-IV: FSIQ	9–13 years, mean 10.5	6 f/8 m	Sigma power	C3, C4	$r = 0.67, p < 0.01$
Lustenberger et al., 2012	ZVT: IQ	18–20 years, mean 19, SD 0.8	15 m	Activity	C4	$r = 0.55, p < 0.05$
Chatburn et al., 2013	SBIS: VIQ	4–13 years, mean 8, SD 2.1	13 f/14 m	Total number: all, fast, slow	C3, C4	NS
Chatburn et al., 2013	SBIS: NVIQ	4–13 years, mean 8, SD 2.1	13 f/14 m	Total number: all, fast, slow	C3, C4	NS
Chatburn et al., 2013	SBIS: FSIQ	4–13 years, mean 8, SD 2.1	13 f/14 m	Total number: all, fast, slow	C3, C4	NS
Chatburn et al., 2013	SBIS: VIQ	4–13 years, mean 8, SD 2.1	13 f/14 m	Density: all, fast, slow	C3, C4	NS
Chatburn et al., 2013	SBIS: NVIQ	4–13 years, mean 8, SD 2.1	13 f/14 m	Density: all, fast, slow	C3, C4	NS
Chatburn et al., 2013	SBIS: FSIQ	4–13 years, mean 8, SD 2.1	13 f/14 m	Density: all, fast, slow	C3, C4	NS
Chatburn et al., 2013	SBIS: VIQ	4–13 years, mean 8, SD 2.1	13 f/14 m	Duration	C3, C4	NS
Chatburn et al., 2013	SBIS: NVIQ	4–13 years, mean 8, SD 2.1	13 f/14 m	Duration	C3, C4	NS
Chatburn et al., 2013	SBIS: FSIQ	4–13 years, mean 8, SD 2.1	13 f/14 m	Duration	C3, C4	NS
Chatburn et al., 2013	SBIS: VIQ	4–13 years, mean 8, SD 2.1	13 f/14 m	Frequency	C3, C4	NS
Chatburn et al., 2013	SBIS: NVIQ	4–13 years, mean 8, SD 2.1	13 f/14 m	Frequency	C3, C4	NS
Chatburn et al., 2013	SBIS: FSIQ	4–13 years, mean 8, SD 2.1	13 f/14 m	Frequency	C3, C4	NS
Gruber et al., 2013	WISC-IV: FSIQ	7–11 years, mean 9, SD 0.9	14 f/15 m	Density	F3, F4, C3, C4, P3, P4, O1, O2	NS
Gruber et al., 2013	WISC-IV: FSIQ	7–11 years, mean 9, SD 0.9	14 f/15 m	Amplitude	F3, F4, C3, C4, P3, P4, O1, O2	NS
Gruber et al., 2013	WISC-IV: FSIQ	7–11 years, mean 9, SD 0.9	14 f/15 m	Duration	F3, F4, C3, C4, P3, P4, O1, O2	NS
Gruber et al., 2013	WISC-IV: FSIQ	7–11 years, mean 9, SD 0.9	14 f/15 m	Frequency	F3, F4, C3, C4, P3, P4, O1, O2	NS
Ward et al., 2014	MAB-II: VIQ	18–29 years, mean 21, SD 3.0	21 f/9 m	Density	C3	$r = 0.18, p > 0.05$
Ward et al., 2014	MAB-II: PIQ	18–29 years, mean 21, SD 3.0	21 f/9 m	Density	C3	$r = 0.14, p > 0.05$
Ward et al., 2014	MAB-II: FSIQ	18–29 years, mean 21, SD 3.0	21 f/9 m	Density	C3	$r = 0.22, p > 0.05$

^aRPMT, Raven Progressive Matrices; APM, Advanced Progressive Matrices; MAB-II, Multidimensional Aptitude Battery-II; SBIS, Stanford-Binet Intelligence Scale; WISC-IV, Wechsler Intelligence Scale for Children IV; WAIS-III, Wechsler Adult Intelligence Scale III; ZVT, Zahlen-Verbindungs-Test; VIQ, verbal IQ; PIQ, performance IQ; FSIQ, full-scale IQ; FIQ, fluid IQ; NVIQ, nonverbal IQ. Data are from Peters et al. (2007, 2008), Ward et al. (2014), and Peters K (personal communication).

Earlier studies on the relationship between sleep spindle parameters and cognition (e.g., Schabus et al., 2006, 2008) have used fixed-amplitude methods for sleep spindle detection (Anderer et al., 2005). These methods do not correct for intraindividual differences in baseline EEG voltage, which on the one hand renders them more sensitive to absolute differences in sleep spindle amplitude, but on the other hand potentially introduces noise due to the influence of non-neural effects (such as skull thickness) on EEG signal amplitude. Despite these differences, our results were successfully, though with weaker effects, replicated using a fixed-amplitude spindle detection algorithm: Both fast spindle amplitude and fast spindle density (technically speaking, the proportion of fast spindles over the critical amplitude) are significantly correlated with IQ in females, but not males.

Although our study is limited in its ability to reveal the precise reason for such sex differences, previous research suggests genetically determined differences in brain anatomy and endocrine function to play a role. On the one hand, sleep EEG features are known to be genetically determined (De Gennaro et al., 2008; Landolt, 2011), and this genetic determination manifests itself largely through variations in brain anatomy and structure (Smit et al., 2012), in which there are notable variations between males and females (Cahill, 2006; Gong et al., 2009; Jazin and Cahill, 2010; Tomasi and Volkow, 2012; Ingahlalikar et al., 2014; Satterthwaite et al., 2014). On the other hand, estrogen and progesterone levels in females, as well as the 2–4 digit ratio (a sensitive correlate of female sex hormones) were shown to be directly associated with sleep spindle features and sleep-related cognitive measures (Driver et al., 1996; Genzel et al., 2012).

Overall, our results only partially confirm previous literature about the positive relationship between intelligence and sleep spindle parameters: We found such positive associations with intelligence for sleep spindle amplitude and sleep spindle length only, and exclusively in females. The focus of many earlier reports of the relationship between sleep spindles and cognitive processes was originally on state markers of sleep-related memory consolidation and not on trait markers, such as intelligence or learning capacity. Such publications of findings originally unintended in the study design have recently been suggested to be prone to publication bias, such as the file drawer effect: results consistent with mainstream views are more probable to be submitted (and accepted), whereas negative findings are mentioned less prominently (Cordi et al., 2014). Indeed, a closer look into the literature reveals a very mixed picture. An early study found fast, but not slow, spindle density to be associated with intelligence (Bódizs et al., 2005). In contrast, three more recent studies did not find significant correlations between fast spindle density and intelligence (Peters et al., 2007, 2008; Ward et al., 2014; K. Peters, personal communication). Of note, however, the former study observed the strongest correlations in frontal and frontopolar regions, whereas the latter analyzed central derivations only. Studies mainly with female participants reported a significant correlation between the total number of sleep spindles and performance IQ but not verbal IQ; however, in one of the samples, this association held only for the upper IQ range (Fogel et al., 2007), and a further study found neither full scale, nor performance, nor verbal IQ to be correlated with sleep spindle σ band (Tucker and Fishbein, 2009). In contrast to these studies, a study with a considerable sample size found spindle duration \times amplitude, but neither total spindle number nor spindle density to be correlated with intelligence (Schabus et al., 2006). Of note, a reanalysis of this study suggests that similar sex differences, as presented here, with a much stronger age-corrected positive cor-

relation between IQ and fast spindle amplitude in females (M. Schabus, personal communication). Although also mental speed as an intelligence-related capacity has been found to correlate with spindle duration \times amplitude (Lustenberger et al., 2012), two studies did not find any correlation between sleep spindle activity and working memory (Limoges et al., 2013; Lafortune et al., 2014), despite being closely associated with fluid intelligence (Conway et al., 2003). Sleep spindle activity has been suggested as a marker of normal intellectual development (Shibagaki et al., 1982); however, in healthy children, a relationship between intelligence and sleep spindles has only been reported for spindle peak frequency (Geiger et al., 2011; Gruber et al., 2013), σ power (Geiger et al., 2012), or not at all (Chatburn et al., 2013).

In sum, only a minority of studies found significant correlations between intelligence and spindle activity (for an overview, see Table 5). Studies with positive results differed markedly in the specific spindle parameters that were correlated with intelligence: number, density, amplitude, length, power, or peak frequency are considered of undifferentiated, slow, or fast sleep spindles (with considerable variability in definitions); some studies further differentiate between the whole night, night halves, thirds, or quarters, and many studies differentially analyzed several EEG derivations. Also, different spindle detection algorithms have been used, with the less sensitive fixed-amplitude spindle detection being most common. In our study, a control analysis with this method has yielded only partially similar results to the IAM spindle detection method; it failed to replicate IAM findings related to slow spindles and spindles on less prominent spindle-generating locations. All in all, the large number of potential spindle variables found in the literature may have potentially led to methodological problems due to multiple comparisons. The above-mentioned publication bias applies in particular to studies with smaller sample sizes and hence low statistical power. All of these problems may have led to false positive or false negative findings in earlier studies.

Most notably, none of the cited studies has targeted potential sex differences, which might have obscured potential correlations. Our results suggest that synaptic plasticity through sleep spindle activity is only one, but not the only possible sleep-related neural mechanism underlying intelligence, and it is mostly present in females, possibly because of their more prominent and functionally more important structural brain connectivity. The general relationship between sleep spindles and intelligence may have been overestimated in the previous literature. Future studies should apply a theoretically grounded and well-defined array of sleep spindle parameters and account for potential sex differences.

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